


## Data Processing of Resting-State fMRI: DPARSF

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## DPARSF

*Frontiers in SYSTEMS NEUROSCIENCE*

METHODS ARTICLE  
published: 14 May 2010  
doi: 10.3389/fnins.2010.00019

### DPARSF: a MATLAB toolbox for “pipeline” data analysis of resting-state fMRI

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Resting-state functional magnetic resonance imaging (fMRI) has attracted more and more attention because of its effectiveness, simplicity and non-invasiveness in exploration of the intrinsic functional architecture of the human brain. However, user-friendly toolbox for “pipeline” data analysis of resting-state fMRI is still lacking. Based on some functions in Statistical Parametric Mapping (SPM) and Resting-State fMRI Data Analysis Toolkit (REST), we have developed a MATLAB toolbox called Data Processing Assistant for Resting-State fMRI (DPARSF) for “pipeline” data analysis of resting-state fMRI. After the user arranges the Digital Imaging and Communications in Medicine (DICOM) files and click a few buttons to set parameters, DPARSF will then give all the preprocessed (slice timing, realign, normalize, smooth) data and results for functional connectivity, regional homogeneity, amplitude of low-frequency fluctuation (ALFF), and fractional ALFF. DPARSF can also create a report for excluding subjects with excessive head motion and generate a set of pictures for easily checking the effect of normalization. In addition, users can also use DPARSF to extract time courses from regions of interest.

**Keywords:** data analysis, DPARSF, REST, resting-state fMRI, SPM

(Yan and Zang, 2010)





## DPARSF

### Data Processing Assistant for Resting-State fMRI (DPARSF)

Yan and Zang, 2010. Front Syst Neurosci.

<http://rfmri.org/DPARSF>

## DPABI

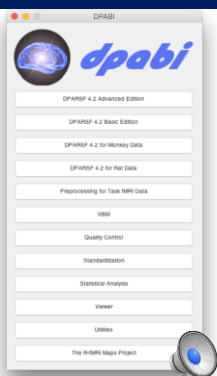

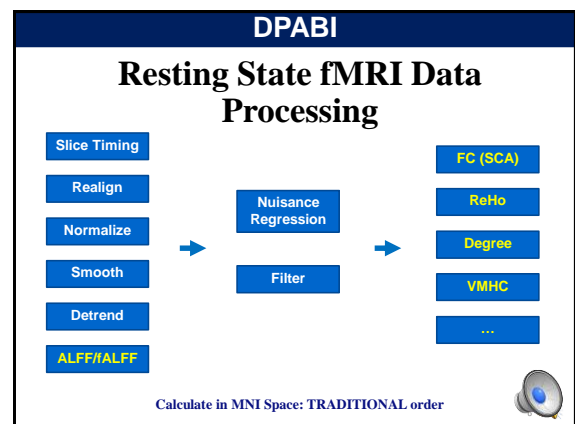
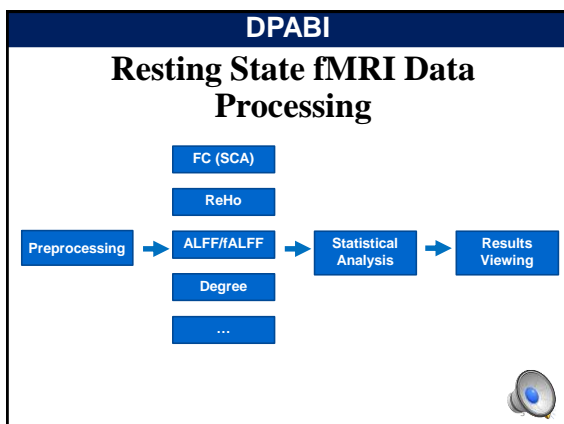
### DPABI: a toolbox for Data Processing & Analysis of Brain Imaging

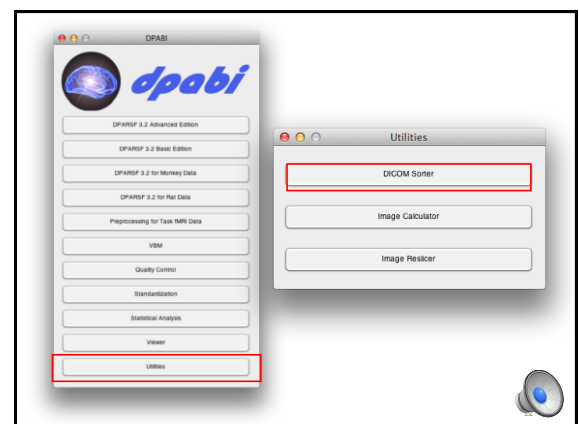
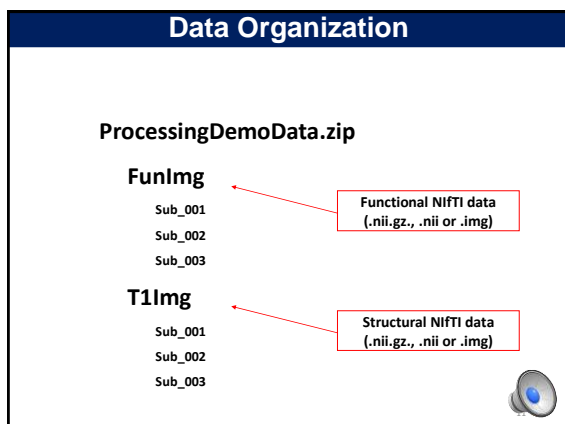
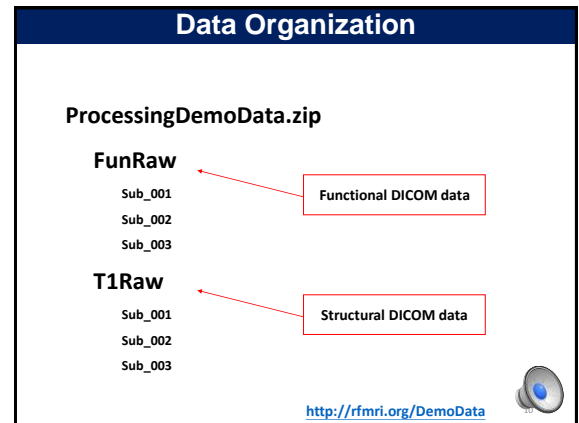
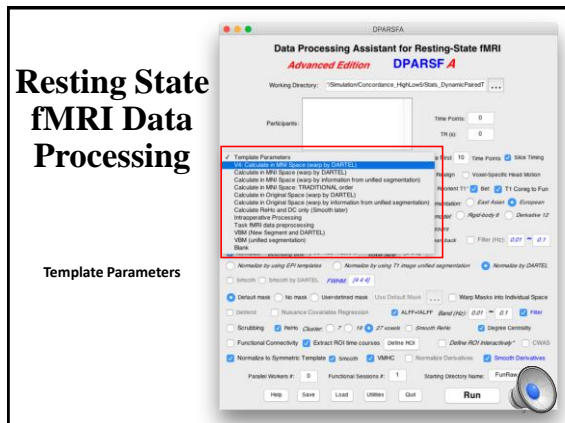
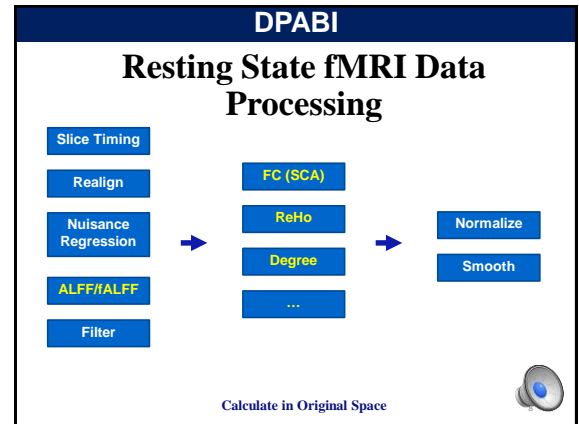
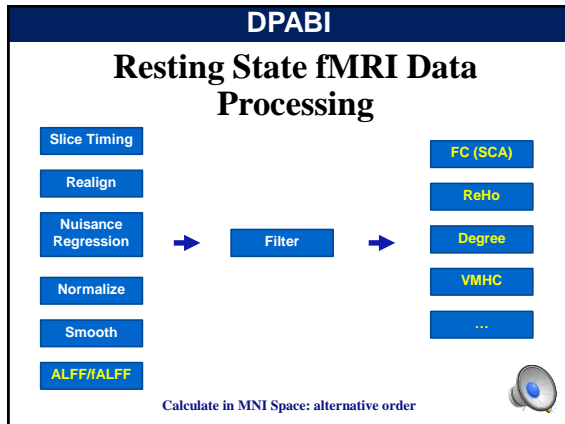
License: GNU GPL

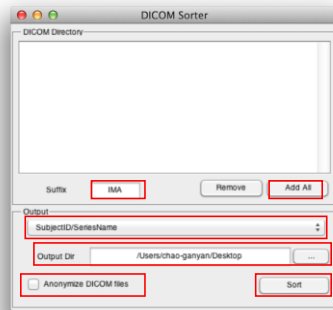
Chao-Gan Yan  
Programmer  
Initiator

Xin-Di Wang  
Programmer

<http://rfmri.org/dpabi>  
<http://dpabi.org>

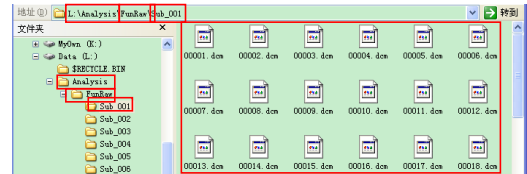






IMA  
dcm  
none

## Data preparation

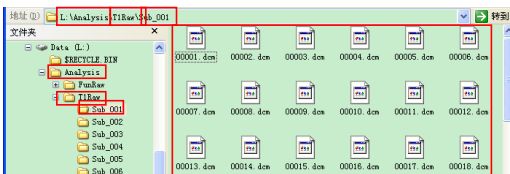
Arrange each subject's fMRI DICOM images in one directory, and then put them in "FunRaw" directory under the working directory.



Subjects' DICOM files directory, please name as this Working directory

## Data preparation

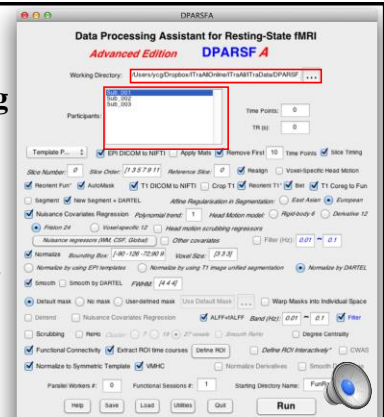
Arrange each subject's T1 DICOM images in one directory, and then put them in "T1Raw" directory under the working directory.



Subjects' T1 DICOM files directory, please name as this Working directory

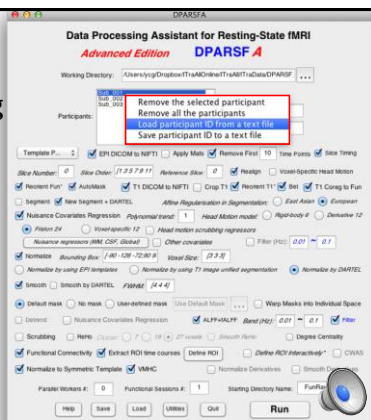
## Preprocessing and R-fMRI measures Calculation

Working Dir where stored Starting Directory (e.g., FunRaw) Detected participants



## Preprocessing and R-fMRI measures Calculation

Detected participants

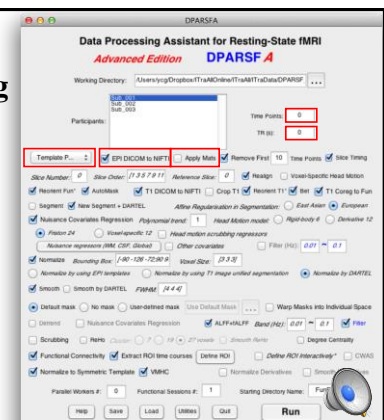


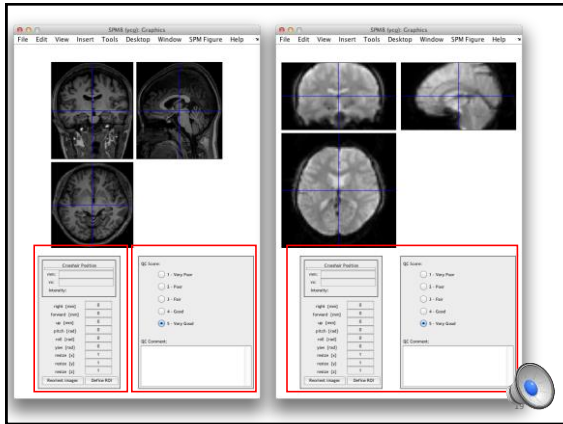
## Preprocessing and R-fMRI measures Calculation

Number of time points (if 0, detect automatically)  
TR (if 0, detect from NIFTI header)

Template Parameters

DICOM to NIFTI, based on MRCroN's Apply reorientation matrices





## Preprocessing and R-fMRI measures Calculation

Apply reorientation matrices:

**ReorientMats**

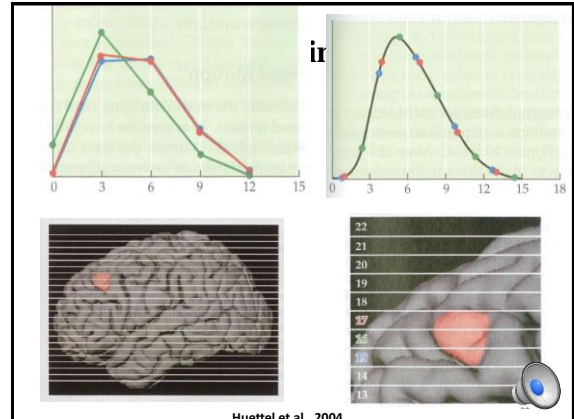
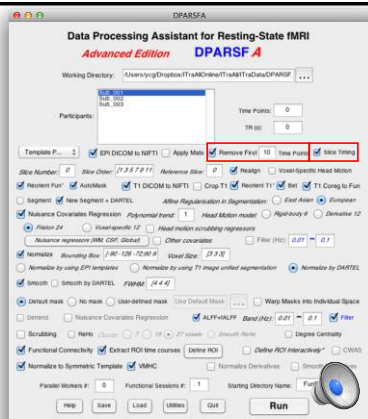
Rename to:

**DownloadedReorientMats**

## Preprocessing and R-fMRI measures Calculation

Remove several first time points

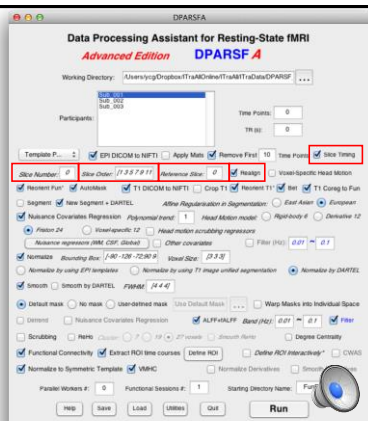
Slice Timing



Huettel et al., 2004

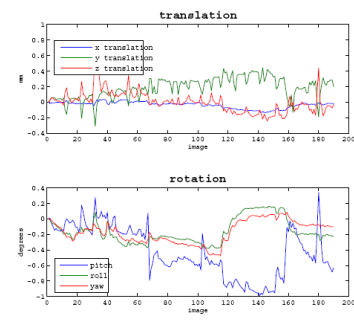
## Preprocessing and R-fMRI measures Calculation

Total slice number  
(if 0, The slice order is then assumed as interleaved scanning:  
[1:2:SliceNumber,2:2:Slice Number]. The reference slice is set to the slice Realign  
slice order at 1:2:33,2:2:32  
(Reference Scanning)  
Slice acquired in the middle time of each R  
CAUTIONS!!!)



## Realign

Why?



## Realign

Check head motion:

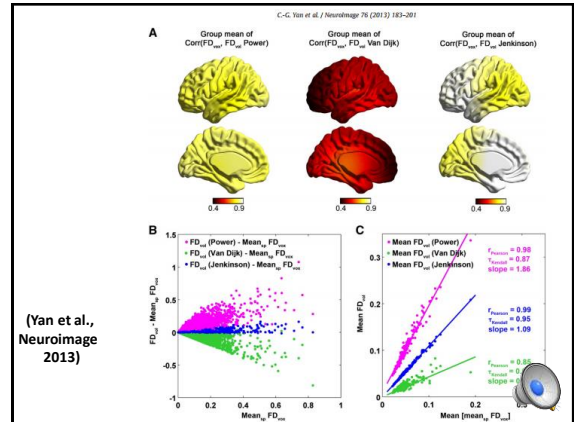
{WorkingDir}\RealignParameter\Sub\_000:

rp\_\*.txt: realign parameters

FD\_Power\_\*.txt: Frame-wise Displacement (Power et al., 2012)

FD\_VanDijk\_\*.txt: Relative Displacement (Van Dijk et al., 2012)

FD\_Jenkinson\_\*.txt: Relative RMS (Jenkinson et al., 2002)



## Realign

Excluding Criteria: 2.5mm and 2.5 degree in max head motion  
None

Excluding Criteria: 2.0mm and 2.0 degree in max head motion  
Sub\_013

Excluding Criteria: 1.5mm and 1.5 degree in max head motion  
Sub\_013

Excluding Criteria: 1.0mm and 1.0 degree in max head motion  
Sub\_007  
Sub\_012  
Sub\_013  
Sub\_017  
Sub\_018



## Realign

Check head motion:

HeadMotion.csv: head motion characteristics for each subject  
(e.g., max or mean motion, mean FD, # or % of FD>0.2)

Threshold:

Group mean (mean FD) + 2 \* Group SD (mean FD)

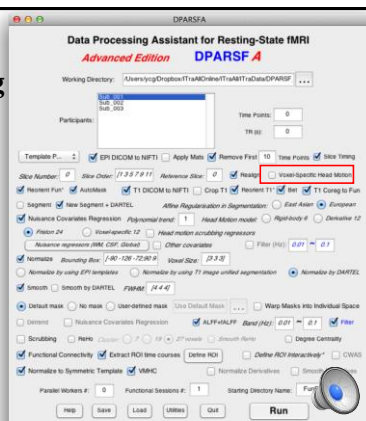
Yan et al., in press Neuroimage; Di Martino, in press, Mol Psychiatry



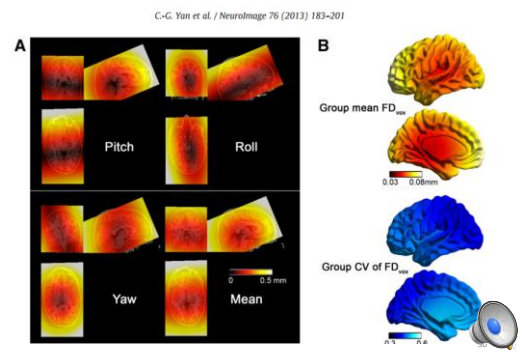
## Preprocessing and R-fMRI measures Calculation

Voxel-Specific Head Motion Calculation

(Yan et al., Neuroimage 2013)



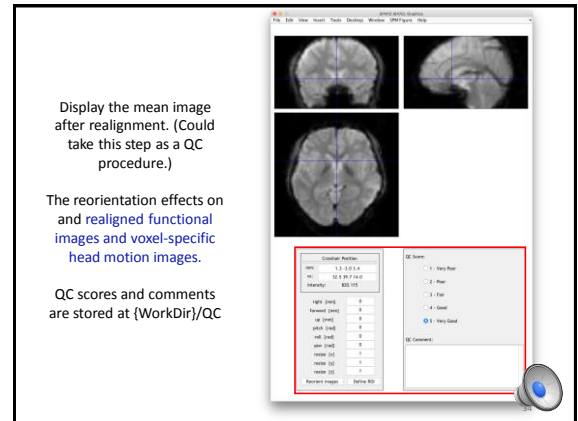
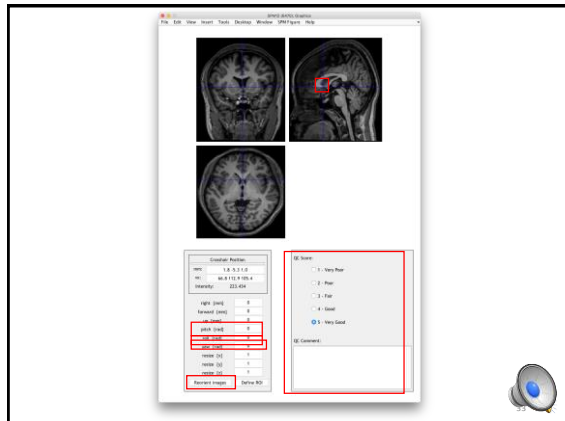
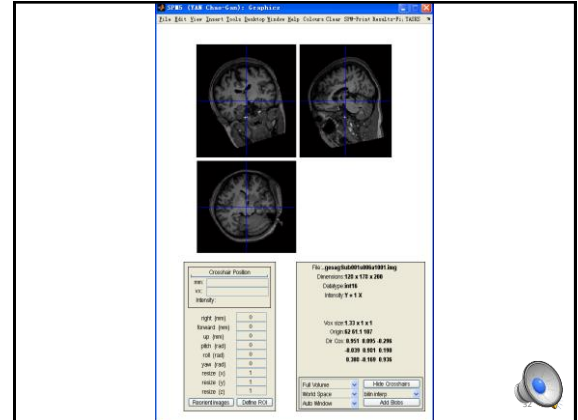
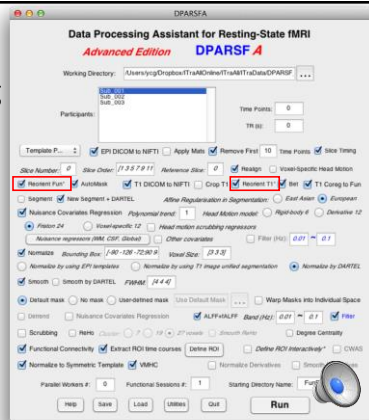
## Voxel-Specific Head Motion Calculation



## Preprocessing and R-fMRI measures Calculation

Reorient Interactively

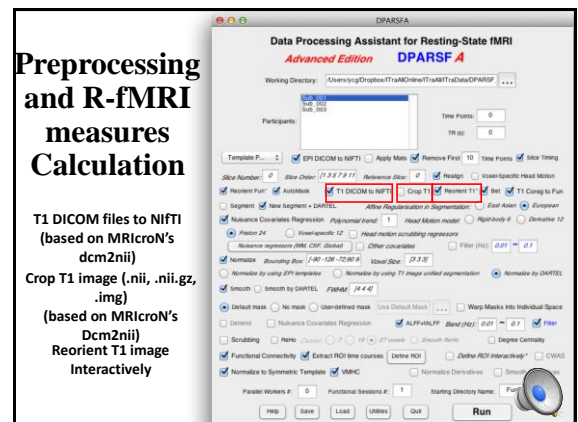
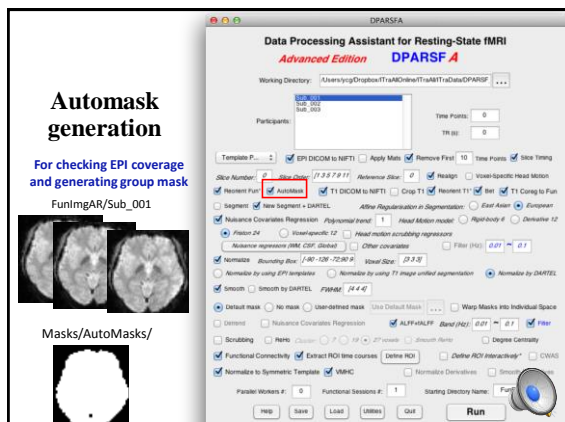
This step could improve the accuracy in coregistration, segmentation and normalization, especially when images had a bad initial orientation. Also can take as a QC step.



Display the mean image after realignment. (Could take this step as a QC procedure.)

The reorientation effects on and realigned functional images and voxel-specific head motion images.

QC scores and comments are stored at (WorkDir)/QC



## Preprocessing and R-fMRI measures Calculation

T1 DICOM files to Nifti (based on MRIcroN's dcm2nii)  
Crop T1 image (.nii, .nii.gz, .img)  
(based on MRIcroN's Dcm2nii)  
Reorient T1 image Interactively

## Brain extraction (Skullstrip)

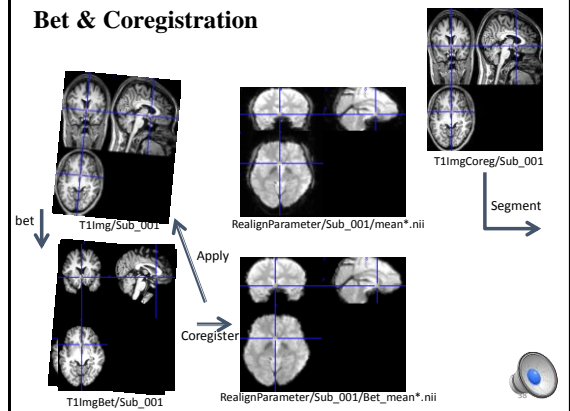
For better coregistration

For Linux and Mac:  
Need to install FSL.

For Windows:  
Thanks to Chris Rorden's  
compiled version of bet  
in MRICron, our  
modified version can  
work on NIFTI images  
directly.



## Bet & Coregistration



## Preprocessing and R-fMRI measures Calculation

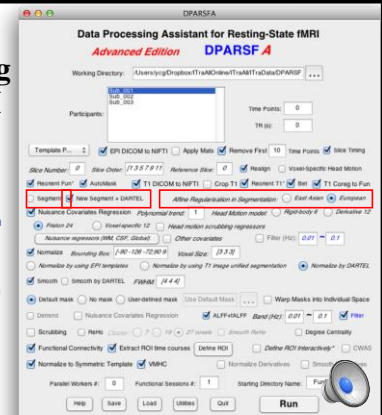
Coregister T1 image to functional space



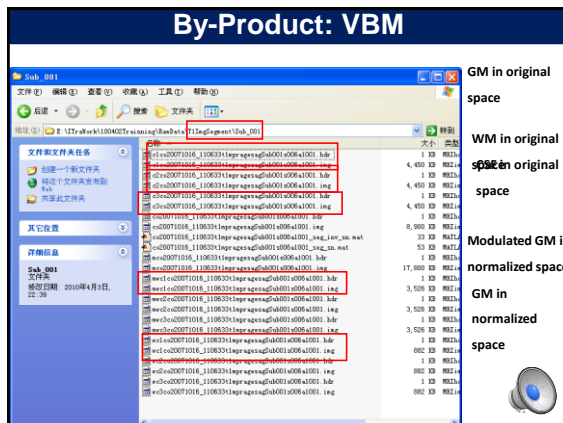
## Preprocessing and R-fMRI measures Calculation

Unified Segmentation.  
Information will be used in  
spatial normalization.  
(In SPM12 and Segment)  
DARTEL

Affine regularisation in  
segmentation



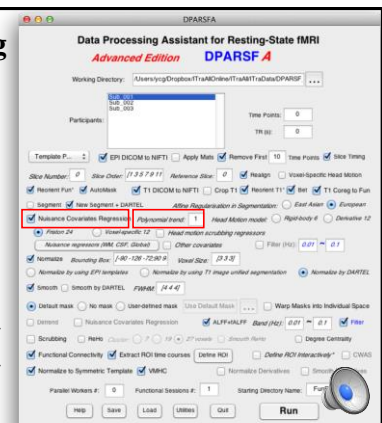
## By-Product: VBM



## Preprocessing and R-fMRI measures Calculation

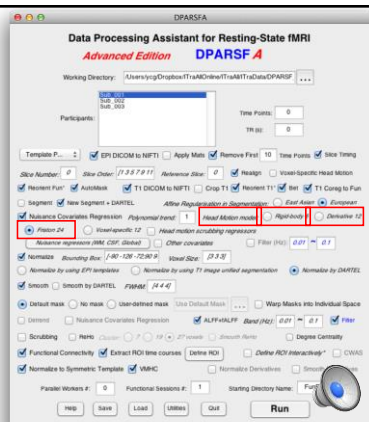
Nuisance Covariates  
Polynomial trends as  
regressors:

- 0: constant (no trends)
- 1: constant + linear trend (same as linear detrend)
- 2: constant + linear trend + quadratic trend
- 3: constant + linear trend + quadratic trend + cubic trend



## Preprocessing and R-fMRI measures Calculation

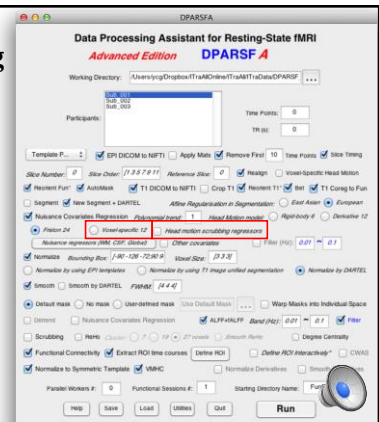
Head Motion regression model  
6 head motion parameters  
Derivatives 12: 6 head motion parameters, 6 first derivatives  
motion parameters one time point before, and the 12 corresponding squared items (Friston et al., 1996).



## Preprocessing and R-fMRI measures Calculation

Voxel-specific 12-parameter model: the 3 voxel-specific translation motion parameters in x, y, z, the same 3 parameters for one time point before, and the 6 corresponding squared items

Head Motion Scrubbing Regressors



Each "bad" time point defined by FD will be used as a separate regressor.



Yan et al., 2013, Neuroimage

Table 3  
Summary recommendations.

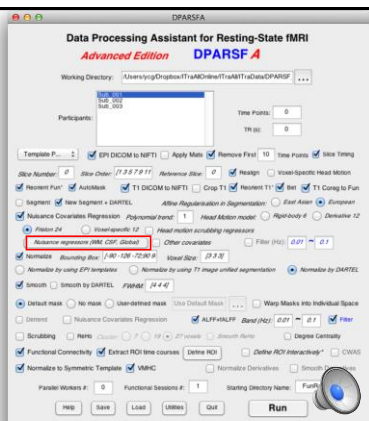
Summary recommendation
<ul style="list-style-type: none"> <li>Individual-level correction with the Friston-24 model is recommended.</li> <li>Additionally, group-level correction for mean FD is recommended, and removes the need for scrubbing.</li> <li>If group-level correction for mean FD is contraindicated or not practical, then individual-level correction with scrubbing is recommended for PCC-FC, VMHC and ReHo (not ALFF, fALFF, DC*).</li> </ul>
Additional considerations
<ul style="list-style-type: none"> <li>Inclusion of global signal regression at the individual-level produces robust reductions in the relationships between motion and R-fMRI measures across participants – particularly for measures without Z-standardization. The benefits of GSR need to be balanced against potential risks for introduction of artifact in the specific analyses employed.</li> <li>For studies limited to low motion datasets, the utility of higher-order Friston 24 model decreases. In this case, we recommend consideration of lower-order (i.e., 6 or 12-parameter) models to minimize the potential for over-fitting, as noted in Satterthwaite et al. (2013).</li> <li>fALFF appeared to be relatively insensitive to motion correction strategies in the present work. Prior work (Satterthwaite et al., 2012) has suggested greater sensitivity in higher motion populations; as such we recommend continued application of correction procedures at the present time.</li> </ul>

\* Recommendations against scrubbing for ALFF and fALFF apply to commonly employed FFT-based implementations (see Limitations and future directions section for alternatives).

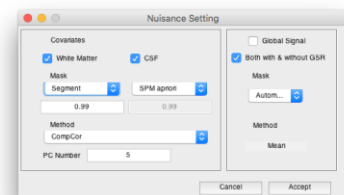
† Recommendations against scrubbing for DC were based on concerns regarding ability to compromise graph construction (see The ability of motion correction strategies to decrease residual relationships between motion and R-fMRI metrics at group-level section for demonstration).

## Preprocessing and R-fMRI measures Calculation

Nuisance Regressors (WM, CSF, Global)



## Nuisance Regression



- Mask based on segmentation or SPM apriori
- CompCor or mean [note: for CompCor, detrend (demean) and variance normalization will be applied before PCA, according to Behzadi et al., 2007]
- Global Signal based on Automask

## Preprocessing and R-fMRI measures Calculation

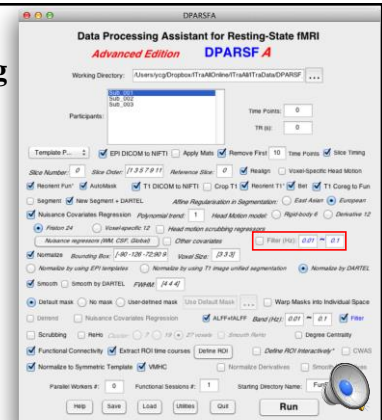
Define other covariates



## Preprocessing and R-fMRI measures Calculation

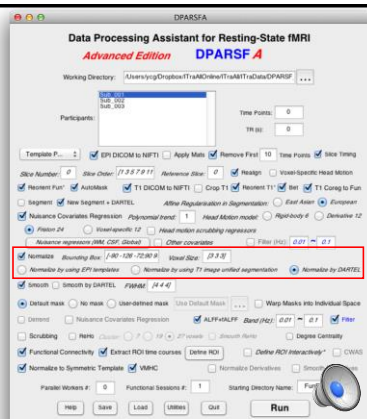
Filtering

The filtering parameters will be used later (Blue checkbox).

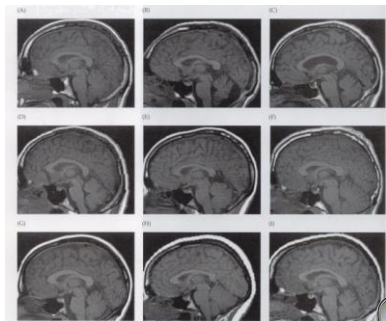


## Preprocessing and R-fMRI measures Calculation

Spatial Normalization



## Normalize



Huettel et al., 2004

## Normalize

Methods:

- I. Normalize by using EPI templates
- II. Normalize by using T1 image unified segmentation
- III. Normalize by using DARTEL
- IV. Normalize by using T1 templates (hidden)

## Normalize

### III. Normalize by using DARTEL

- ❖ Structural image was coregistered to the mean functional image after motion correction
- ❖ The transformed structural image was then segmented into gray matter, white matter, cerebrospinal fluid by using a unified segmentation algorithm (New Segment)
- ❖ DARTEL: create template
- ❖ DARTEL: Normalize to MNI space. The motion corrected functional volumes were spatially normalized to the MNI space using the normalization parameters estimated in DARTEL.

## Preprocessing and R-fMRI measures Calculation

Smooth

For ReHo, Degree Centrality: don't smooth before calculation

FWHM kernel settings can be applied to later steps



## Smooth

Why?

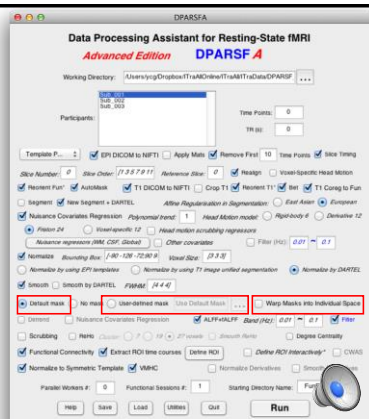
- Reduce the effects of bad normalization
- Increase SNR
- ...



## Mask

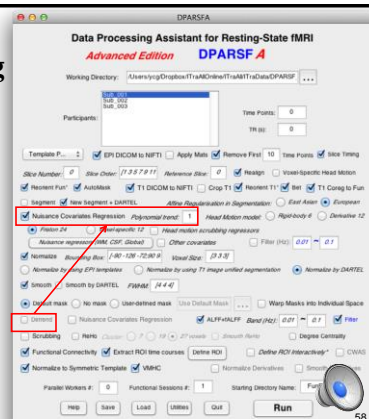
Default mask: SPMS apriori mask (brainmask.nii) thresholded at 50%. User-defined mask

Warp the masks into individual space by the information of DARTEL or unified segmentation.



## Preprocessing and R-fMRI measures Calculation

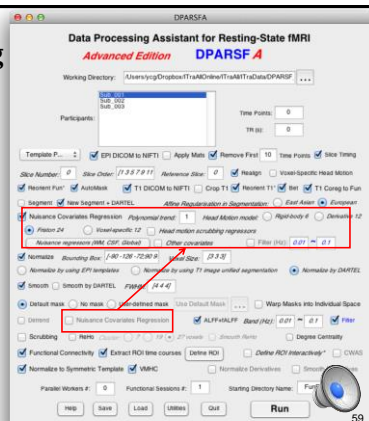
Linear detrend (NO need since included in nuisance covariate regression)



## Preprocessing and R-fMRI measures Calculation

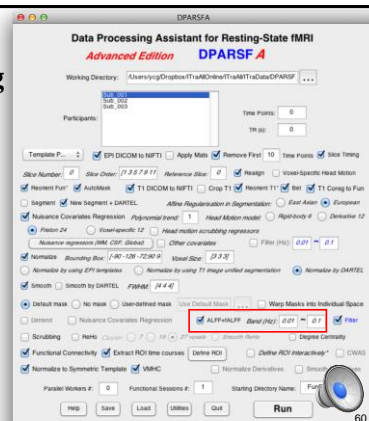
Nuisance Covariates Regression

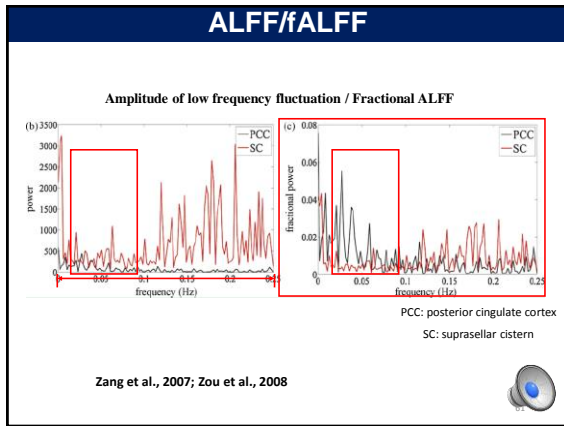
If needed, then use the parameters set in the upper section.



## Preprocessing and R-fMRI measures Calculation

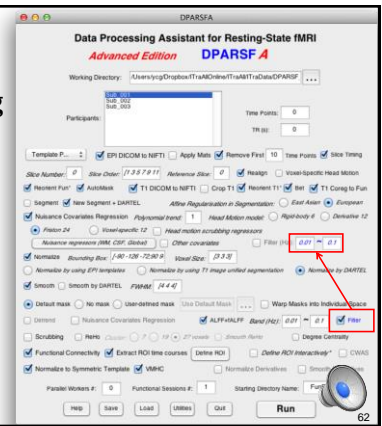
ALFF and fALFF calculation (Zang et al., 2007; Zou et al., 2008)





## Preprocessing and R-fMRI measures Calculation

Filtering  
Use the parameters set in the blue edit boxes.



## Preprocessing and R-fMRI measures Calculation

Scrubbing

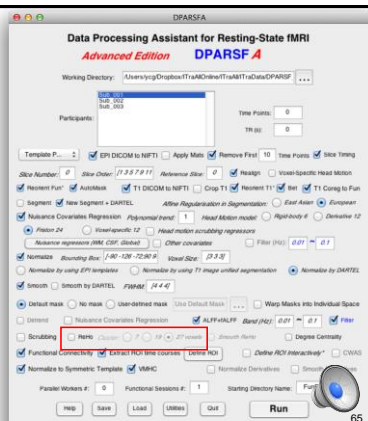


The "bad" time points defined by FD\_Power (Power et al., 2012) will be interpolated or deleted as the specified method.

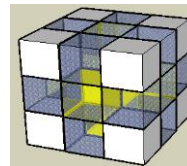


## Preprocessing and R-fMRI measures Calculation

Regional Homogeneity (ReHo) Calculation (Zang et al., 2004)



## ReHo (Regional Homogeneity)



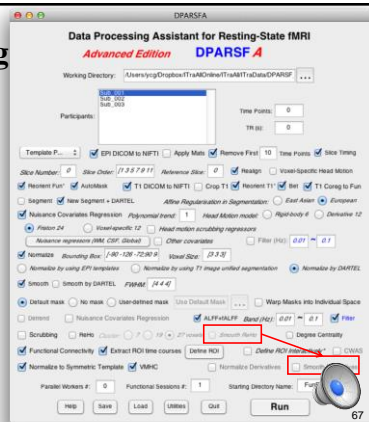
$$W = \frac{\sum (R_i)^2 - n(\bar{R})^2}{12 K^2 (n^3 - n)}$$

Zang et al., 2004

Zang YF, Jiang TZ, Lu YL, He Y, Tian LX (2004) Regional homogeneity approach to fMRI data analysis. Neuroimage 22: 39.

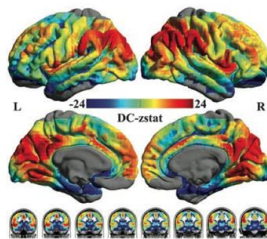
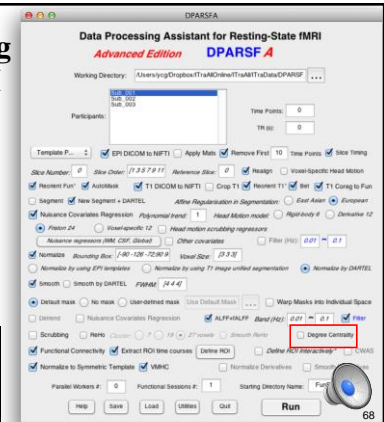
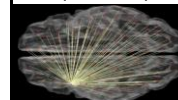
## Preprocessing and R-fMRI measures Calculation

Regional Homogeneity (ReHo) Calculation (Zang et al., 2004)



## Preprocessing and R-fMRI measures Calculation

Degree Centrality Calculation (Buckner et al., 2009; Zuo et al, 2012)  
> r Threshold (default 0.25)



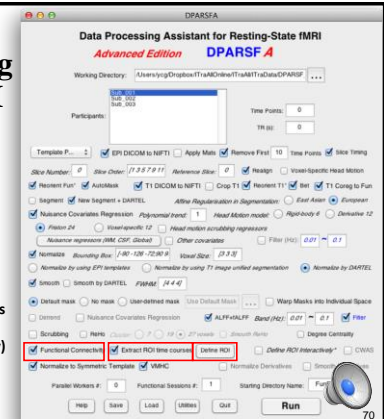
Zuo et al., 2012

## Preprocessing and R-fMRI measures Calculation

Functional Connectivity (voxel-wise seed based correlation analysis)

Extract ROI time courses (also for ROI-wise Functional Connectivity)

Define ROI



## Define ROI

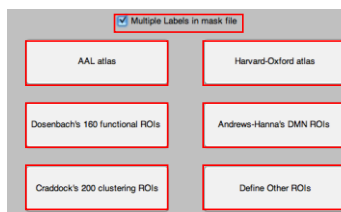
Multiple labels in mask file: each label is considered as one ROI

Dosenbach et al., 2010

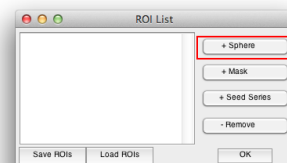
Andrews-Hanna et al., 2010

Craddock et al., 2011

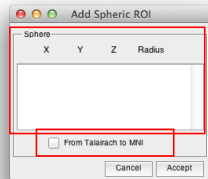
Define other ROIs



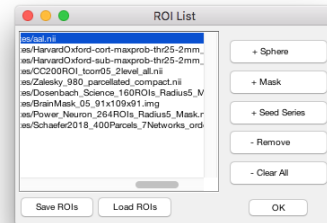
## Define ROI



## Define ROI

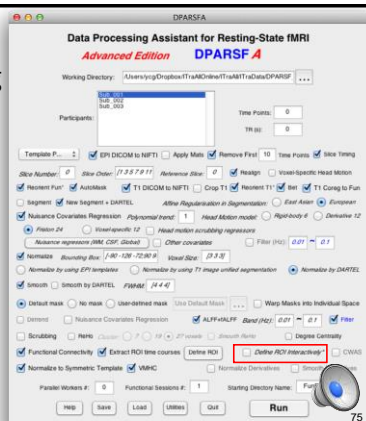


## Define ROI

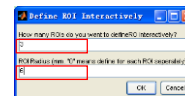


## Preprocessing and R-fMRI measures Calculation

Define ROI Interactively

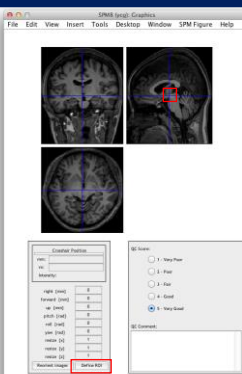


## Define ROI



0 means define ROI Radius for each ROI separately

## Define ROI



## Functional Connectivity

You will get the Voxel-wise functional connectivity results of each ROI in {working directory}\Results\FC:

zROI1FCMap\_Sub\_001.img

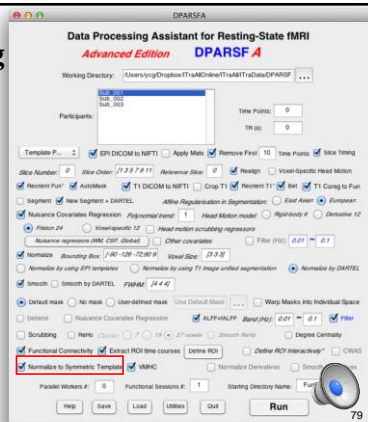
zROI2FCMap\_Sub\_001.img

For ROI-wise results, please see {working directory}\Results\FunMapARCW\*\_ROISignals.

## Preprocessing and R-fMRI measures Calculation

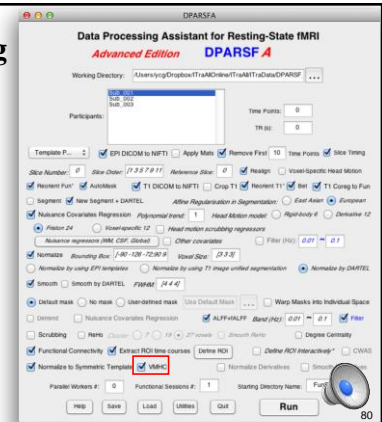
Voxel-mirrored homotopic connectivity (VMHC) (Zuo et al., 2010)

Prepare for VMHC: Further register to a symmetric template



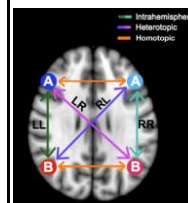
## Preprocessing and R-fMRI measures Calculation

Voxel-mirrored homotopic connectivity (VMHC) (Zuo et al., 2010)

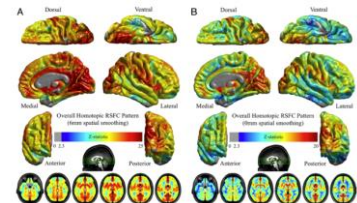


## VMHC

- 1) Get the T1 images in MNI space (e.g., wco\*.img or wco\*.nii under T1ImgNewSegment or T1ImgSegment) for each subject, and then create a **mean T1 image template** (averaged across all the subjects).
- 2) Create a **symmetric T1 template** by averaging the mean T1 template (created in Step 1) with its flipped version (flipped over x axis).
- 3) **Normalize the T1 image in MNI space** (e.g., wco\*.img or wco\*.nii under T1ImgNewSegment or T1ImgSegment) for each subject to the **symmetric T1 template** (created in Step 2), and **apply the transformations to the functional data** (which have been normalized to MNI space beforehand). Please see a reference from Zuo et al., 2010.



Gee et al., 2011

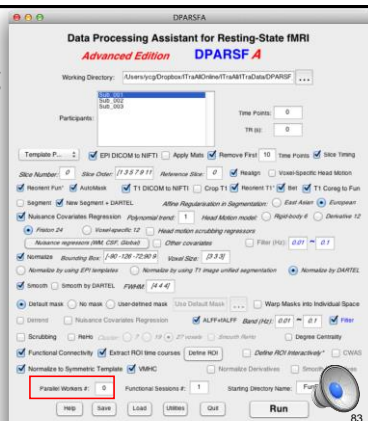


Zuo et al., 2010

## Preprocessing and R-fMRI measures Calculation

Parallel Workers (if parallel computing toolbox is installed)

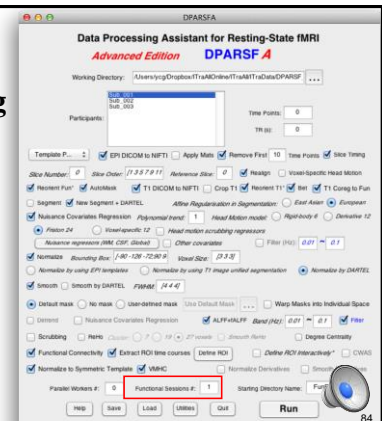
Each subject is distributed into a different worker. (Except DARTEL-Create Template)



## Preprocessing and R-fMRI measures Calculation

Multiple functional sessions

1<sup>st</sup> session: FunRaw  
2<sup>nd</sup> session: S2\_FunRaw  
3<sup>rd</sup> session: S3\_FunRaw  
...



## Starting Directory Name

If you do not start with raw DICOM images, you need to specify the Starting Directory Name.

E.g. "FunimgARW" means you start with images which have been slice timed, realigned and normalized.

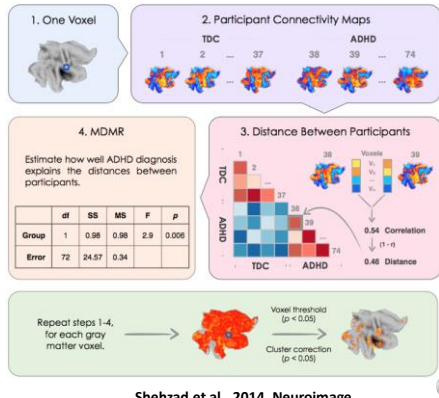
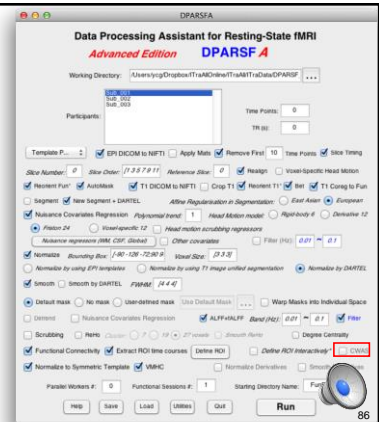
S - Smooth  
D - Detrend  
F - Filter  
C - Covariates Removed  
B - Scrubbing



## Preprocessing and R-fMRI measures Calculation

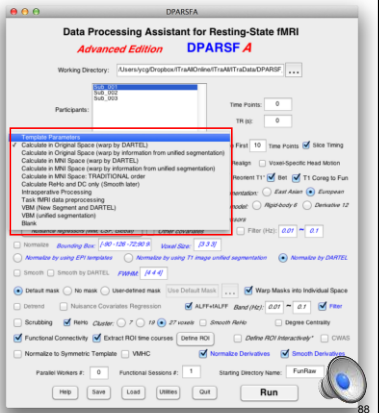
Connectome-wide association studies based on multivariate distance matrix regression (Shehzad et al., 2014)

Resource consuming as compared to other measures



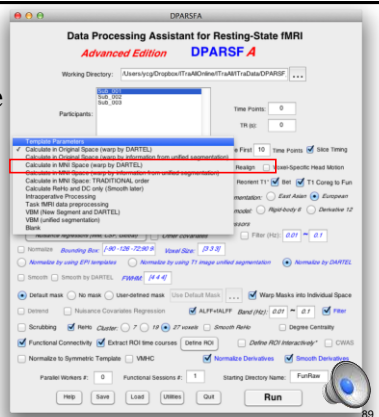
## Resting State fMRI Data Processing

Template Parameters



## Resting State fMRI Data Processing

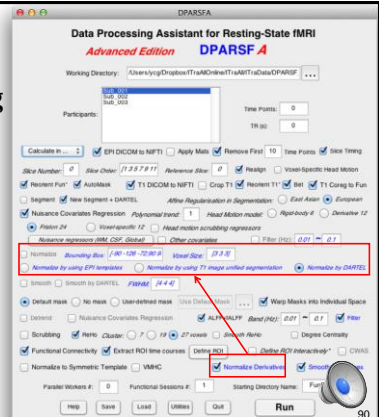
Calculate in MNI space  
Calculate in Original space



## Preprocessing and R-fMRI measures Calculation

Normalize measures (derivatives) calculated in original space into MNI space

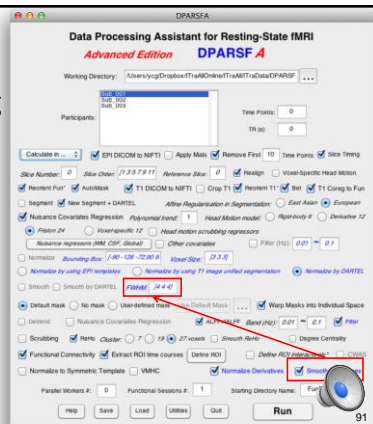
Use the parameters set in the upper section.



## Preprocessing and R-fMRI measures Calculation

Smooth R-fMRI measures (derivatives)

Use the parameters set in the upper section.



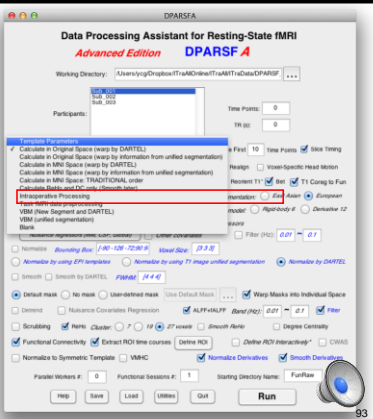
## Preprocessing and R-fMRI measures Calculation

Warp masks into original space



## Resting State fMRI Data Processing

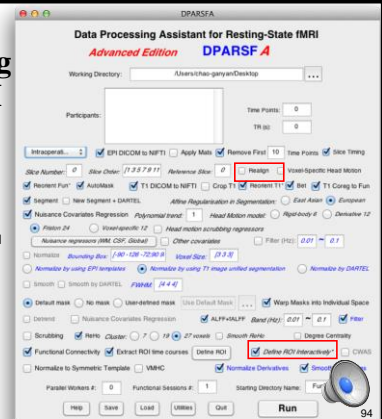
Intraoperative Processing



## Preprocessing and R-fMRI measures Calculation

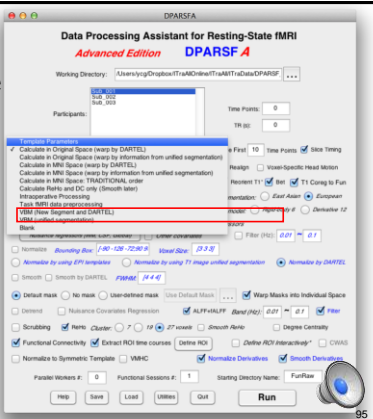
No realign since there is no head motion. DPARSFA will generate the mean functional images automatically.

Define ROI Interactively



## Resting State fMRI Data Processing

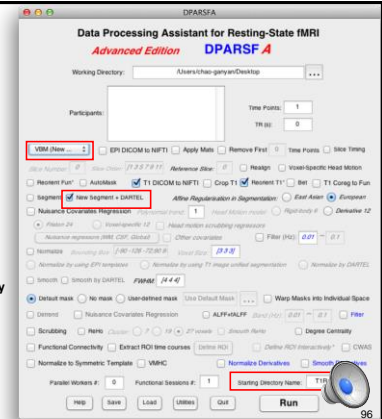
VBM



## VBM

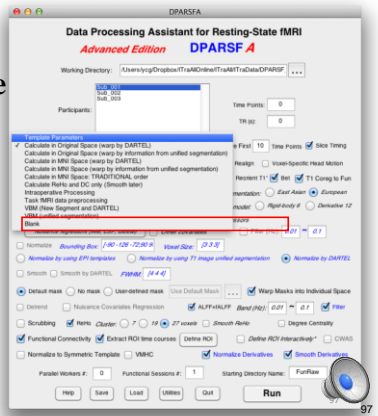
Only New Segment + DARTEL is checked

Define the Starting Directory Name as T1Raw



## Resting State fMRI Data Processing

Blank



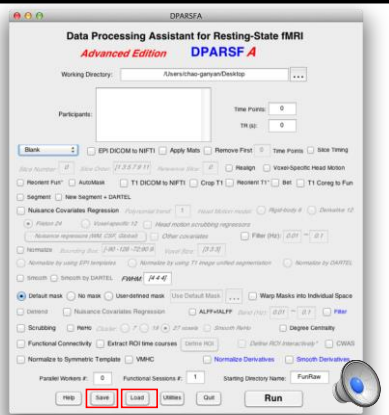
Blank



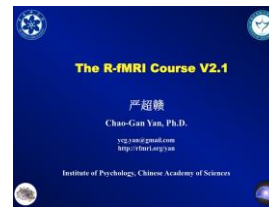
## Save and Load Parameters

Save parameters to \*.mat

Load parameters from \*.mat



## Further Help



<http://rfmri.org/Course>



<http://rfmri.org/wiki>

The R-fMRI Journal Club



Official Account: RFMRILab

## Preprints of the R-fMRI Network



Preprints of the R-fMRI Network (PRN) is a preprint, open-access, free-submission, open-discussion, community funded Preprints of R-fMRI related research. The goal of PRN is to supplement the peer reviewed journal publication system – by more rapidly communicating the latest research achievements across the global.

F1000Research

F1000Research 2018, 8:122 (last updated 21 AUG 2019)



### SOFTWARE TOOL ARTICLE

**REVIEWED** PRN: a preprint service for catalyzing R-fMRI and neuroscience related studies [v2; ref status: indexed, <http://f1000r.es/5qy>]

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## 数据分析与深度培训



### 静态功能磁共振成像深度数据分析

功能磁共振成像越来越成为一种主流的科研手段，然而功能磁共振的数据分析却是一项具有高度挑战性的工作。海量的原始数据，繁多的分析步骤，复杂的分析方法都让研究者们无所适从，恰当的分析方法可以从海量的数据中挖掘出富有创新性的结果，而不恰当的分析则可能让精心收集的数数据黯然失色。深度大脑公司联合中国科学院 The R-fMRI Lab 的专业功能磁共振研究团队，推出一站式功能磁共振数据分析解决方案，助您从容应对功能磁共振数据带来的挑战。



<http://deepbrain.com>

### 静态功能磁共振成像数据深度处理培训

从您见到这条消息开始，您便将有与中国科学院 The R-fMRI Lab 的静态功能磁共振专家团队共同探索大脑的奥秘！深度跟组培训期间，您将亲身体验：

- 数据处理：专家指导下高效学习静态功能磁共振成像数据处理；
- 思路设计：与国际知名专家讨论研究思路；
- 论文撰写：系统的 SCI 论文写作训练。

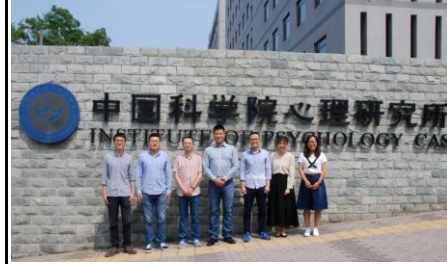
## The R-fMRI Lab



WeChat Official Account: RFMRILab



## Acknowledgments



Chinese Academy of  
Sciences  
Xi-Nian Zuo  
Hangzhou Normal  
University  
Yu-Feng Zang  
NYU Child Study Center  
F. Xavier Castellanos  
  
Child Mind Institute  
Michael P. Milham

### Funding

- National Natural Science Foundation of China
- National Key R&D Program of China
- Chinese Academy of Sciences



**Thanks for your attention!**

